3-Dimensional Printing in Transcatheter Aortic Valve Replacement: Periprocedural Value and Training Applications

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Abstract

Review

Transcatheter aortic valve replacement (TAVR) is a rapidly developing, cutting-edge technology. The skills to perform such procedures are difficult to acquire, and the learning curve is steep. In recent years, structural heart diseases, particularly valvular disease, have become one of the main areas to which 3-dimensional (3D) printing has been applied because it facilitates visualization and exploration of complex cardiovascular anatomical structures. 3D printing also addresses some of the challenges of these interventions, such as patient selection, prosthesis sizing, and of course, teaching and training. 3D printing can provide a valuable resource for teaching and training because it can produce educational models for all types of valvular diseases. A pulsatile platform for the simulation of TAVR with 3D printed models could be used for comprehensive training of young clinicians as part of the overall TAVR teaching and training program. In this review, we introduced the 3D printed model and TAVR simulator, illustrate its training applications in morphology teaching, surgical simulations and preprocedural planning. Additionally, we reviewed studies on 3D printing in predicting periprocedural complications of TAVR, discussed the current limitations and prospected future directions of 3D printing.

Keywords

transcatheter aortic valve replacement; 3D printing; models; teaching; training

Introduction

After twenty years of development, a large amount of evidence-based research has reinforced the idea that transcatheter aortic valve replacement (TAVR), as a leading and revolutionary technology, is changing the treatment strategy and direction of aortic valve diseases, which leads to less trauma, lower risk, faster recovery speed and better prognosis in patients [1–3]. However, the difference between TAVR and surgical aortic valve replacement (SAVR)

lies in the fact that it is difficult to look directly at the full view of the aortic root, let alone to open the heart to observe the internal anatomic structures [4]. With the continuous development of medical visualization, digital modeling is required to be increasingly accurate, and the requirement of precision is particularly important in cardiovascular diseases [5]. Advances in 3-dimensional (3D) printing have proven its value and potential in many fields, in particular by opening up new approaches for the diagnosis and treatment of many complex cardiovascular diseases. Clinicians who specialize in diagnostic and interventional radiology could use imaging data to complete 3D reconstructions and models and to provide the surgeons with clear models of the individualized anatomical structures [6-8]. These clinicians collect the patients' preprocedural computed tomography angiography (CTA) imaging data to reconstruct 3D models and use the 3D printer to create individualized models [9,10]. The models provide clinicians with intuitive anatomical structures to assist with surgical training, preprocedural planning, and intraprocedural guidance and also play an integral role in medical education and training [11,12].

Furthermore, 3D printed models are already available for various applications, especially for training purposes. Studies have demonstrated the importance of hands-on participation and instruction in stimulating the interest of medical students in becoming surgeons [13–16]. This trend is driven by the desire to improve the quality of patient care and ensure patient safety [17]. A major advantage of simulation is that it creates a valuable practice environment for students [17]. The combination of 3D printing and transcatheter aortic valve replacement (TAVR) allows doctors to view the anatomical structures directly through the 3D printed models, which may also improve the communication between doctors and patients and train young clinicians and medical students as well [18,19]. Although the simulation-based mode has been widely accepted, it has not been applied in many areas of medicine in which educational needs exist. Therefore, in this review, we discussed recent advances and specific applications, especially training applications, of 3D printing in TAVR from a technical perspective.

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3-Dimensional Aortic Valve Printed Model and Simulator

The process of creating an individualized 3D printed model is completed in 4 steps: (1) Clinical imaging: the medical image data are acquired; (2) image segmentation: the region of interest is extracted, reconstructed, and then printed; (3) data transformation: the volumetric data are transformed into a model recognizable for 3D printing; (4) model printing: the digital model is imported into a 3D printer for printing. Post-processing procedures, such as removal of support structures, grinding, clarifying, and polishing, produce an exquisite, colorful multimaterial 3D model for clinical use.

3-Dimensional Printed Models Generated by Multimodality Imaging

CTA is commonly used in cardiovascular diseases to provide high-quality images through angiography and is the preferred data source for 3D printing of cardiac anatomical structures. Computed magnetic resonance (CMR) has certain advantages over CTA in the display of valves and adjacent tissues, but the application is somewhat limited because it is time-consuming. With the development of echocardiography, the spatial and temporal resolution of images has increased significantly and could also be used for 3D reconstructions. These acquired images are then converted to the standard format for Digital Imaging and Communications in Medicine for storage.

First, the patient's computed tomography (CT) data are imported into Materialise Mimics version 21.0 software (Materialise, Leuven, Belgium). Three orthogonal sections (coronal, sagittal, and cross-sectional) are created by using interactive multiplanar imaging reconstruction. After comparison and confirmation of the 3D reconstruction, the outlined area is reconstructed to obtain the initial 3D model of the aortic root. Second, Materialise 3-matic software (Materialise, Leuven, Belgium) is used to fully reconstruct the morphology of the aortic root and the distribution of the calcified areas. Different colors are used to differentiate the parts in the digital model that exemplify the multidimensional structural information, such as the morphology, distribution, and junctions of each part. The digital model is then exported into Standard Tessellation Language format. Finally, the Standard Tessellation Language files are imported into a Polyjet 850 multimaterial full-color 3D printer (Stratasys, Inc., Eden Prairie, MN, USA). Different materials are selected to represent the different tissues [20-22] (Fig. 1).

Pulsatile Platform for the Simulation of Transcatheter Aortic Valve Replacement

Conventional in vitro tests rely on static models that do not truly reflect the pathophysiological characteristics of the heart. By assembling a pulsatile platform for simulation, the individual 3D printed models of the aortic root and adjacent tissues are used to simulate cardiac motion in the diseased structures [23,24]. The 3D printed models, such as those for aortic stenosis with calcification and aortic valve prolapse with regurgitation, closely simulate the actual physiological environment. At the same time, measurements are taken using high-speed cameras, X-ray equipment, and echocardiography to simulate TAVR and to obtain data similar to the clinical data. Data analysis and comparisons may optimize all aspects of the TAVR procedure, including the hemodynamic characteristics of the aortic valve (e.g., incomplete valve expansion due to valve calcification), further improving the efficacy and reliability of the operation. The platform may help young clinicians develop an intuitive understanding of TAVR, rapidly improve their learning curves, and avoid the occurrence of future complications [25-27] (Fig. 2 and Supplementary Video 1).

Current Teaching and Training Applications in Transcatheter Aortic Valve Replacement

3D printed models of different types of aortic valve diseases are used to educate and train young clinicians and medical students to fully appreciate the reconstructed anatomical structures of the aortic root prior to the procedure and to practice procedural simulations using the models. Applying 3D printing in TAVR for the evaluation of complications is a new concept [28,29]. It is of great significance in helping young clinicians and medical students understand the structural changes that can occur in various types of aortic valve diseases and to deepen their knowledge of the anatomical and pathophysiological characteristics of diseases. In addition, it contributes to reducing the use of experimental animals and improving animal welfare.

Morphology Teaching

An accurate understanding of aortic valve diseases is essential for diagnosis and treatment. The teaching of valve morphology has traditionally relied mainly on the observation of pathological specimens removed from deceased patients or of heart transplants. Although the surgical outcomes continue to improve, sources of new specimens are becoming increasingly rare due to the ethical and legal issues associated with retaining human or body parts for educational purposes [30]. Unlike actual specimens that can be cut into a limited number of dissections, the 3D printed models can be replicated in any number of dissections to fully demonstrate the complex anatomical structures and

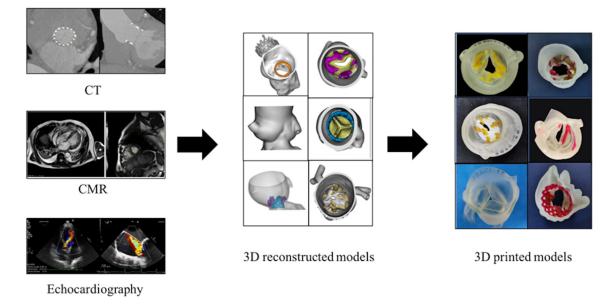


Fig. 1. The printing process for 3-dimensional models. CT, computed tomography; CMR, computed magnetic resonance; 3D, 3-dimensional.

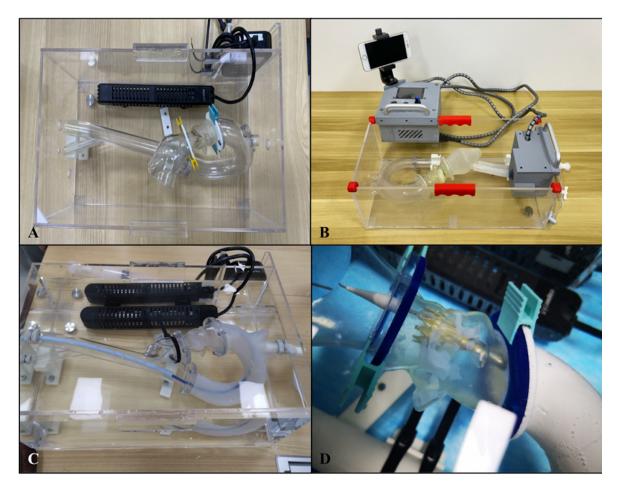


Fig. 2. The pulsatile platform for the simulation of transcatheter aortic valve replacement (TAVR) using 3-dimensional printed models. (A) Multiapproach TAVR simulator; (B) Transcatheter femoral artery TAVR simulator; (C) The TAVR simulation process; and (D) Stent expansion.



Fig. 3. Teaching by using 3-dimensional (3D) printed models. (A) An experienced physician teaches young clinicians about the morphology of the aortic root using a 3D printed model. (B) An experienced physician teaches trainees using a model combined with echocardiography.

thus provide a more intuitive understanding of the aortic root, including its morphology, size, and position; the structures of the adjacent tissues; and clear examples of aortic valve stenosis or regurgitation, leaflet calcification, and the distribution of calcification (Fig. 3).

Surgical Simulation

TAVR training is very important for the growth of young clinicians. With the rapid development of imaging, bioengineering, and digital modeling, a training system based on 3D printing provides more training opportunities. Through virtual surgical design and hemodynamic simulation, 3D printing can display and predict quantitative changes in hemodynamic parameters during surgery, providing reliable information for reducing surgical risks. As 3D printing continues to improve, the individualized aortic root model can be printed, allowing trainees to obtain an intuitive impression of the anatomical structures of a specific patient.

To closely simulate TAVR, the aortic root model is placed in a pulsatile platform. From there, all kinds of connections and covert attachments are established to formulate a TAVR training device. Young clinicians may use the device to practice skills such as threading across the annulus, exchanging the guidewire, and positioning the stent, all of which will improve operating skills and proficiency to promote more rapid movement along the learning curve (Fig. 4 and **Supplementary Videos 2,3**).

Preprocedural Planning

3D printing is not only consistent in its production of surgical models but it also provides a new approach for surgical training. The individual model printed by 3D reconstruction may assist doctors in understanding the patient's individual anatomical structures more intuitively and provide clinical help for determining the patient's preprocedural planning. Olivieri *et al.* [31] reported that different types of stents were tried on the 3D printed model before the operation for a patient diagnosed with complete transposition of the arteries accompanied by right pulmonary vein obstruction. Appropriate stents were selected for successful treatment due to the advantages of clearly displaying the positions of the arteries [31], which led to successful treatment outcomes. Hermsen *et al.* [32] used the 3D model of hypertrophic cardiomyopathy to simulate the operation.

Prediction of Transcatheter Aortic Valve Replacement Complications

Paravalvular Leakage

Paravalvular leakage refers to the regurgitation of blood flow to the left ventricle during ventricular diastole, which is one of the most common complications after TAVR [33]. Qian *et al.* [34] successfully used the 3D printed model of the aortic root to predict the incidence of paravalvular leakage during TAVR [35,36]. Preprocedural simulation with the 3D printed model of the aortic root can accurately show the position and severity of the possi-

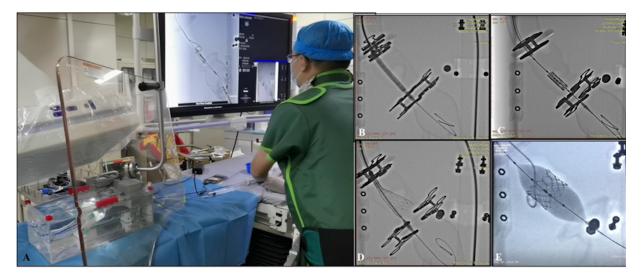


Fig. 4. Simulation of transcatheter aortic valve replacement (TAVR) in the catheterization laboratory using the 3-dimensional (3D) printed models, the pulsatile simulator, and different TAVR devices. (A) An experienced surgeon demonstrates the simulated TAVR procedure. (B) A simulating device passes through the 3D printed model using a self-expandable TAVR system. (C) A simulating device passes through the 3D printed model using a balloon-expandable TAVR system. (D) Simulating the release of the TAVR device in the 3D printed model using a self-expandable TAVR system. (E) Simulating the release of the TAVR device in the 3D printed model using a balloon-expandable TAVR system.

ble paravalvular leakage, which may help young clinicians choose different types of prosthetic valves (Fig. 5A,B).

Conduction Block

After TAVR, the atrioventricular conduction system at the junction between the right coronary sinus and the noncoronary sinus may be continuously suppressed or permanently damaged due to displacement of the calcification, and the prosthetic valve may also damage the conduction system, which is positioned in the interventricular septum. Therefore, 3D printing can be used to print a model of aortic stenosis with the calcified areas, which, when combined with the measured data, can be used to choose the correctly sized balloon-expandable valve to help young clinicians estimate the migrated direction of the balloon. Rocatello et al. [37] demonstrated that 3D reconstruction of the aortic root is clinically significant because it reduces the incidence of postprocedural conduction block. In addition, different stents could be selected to simulate TAVR, stents which, when influenced by calcification, could be observed to migrate in a particular direction. The young clinicians could then estimate the probability of conduction block (Fig. 5C,D).

Coronary Obstruction

Coronary obstruction refers to the phenomenon of myocardial infarction after the stent exerts pressure on the valve or on the calcification to the coronary artery after TAVR or during the long-term follow-up period. Heitkemper *et al.* [38] showed that reconstructing the aortic root by 3D printing preoperatively allowed them to demonstrate the distribution of the calcification to avoid the occurrence of coronary obstruction [39]. For patients with a high risk of coronary obstruction, 3D printing can be used to print the aortic root model, and the model could be used to simulate balloon expansion *in vitro*, which may help young clinicians estimate the possibility of coronary obstruction after TAVR (Fig. 5E,F).

Vascular Complications

The approaches for TAVR are now mainly divided into the peripheral vascular approach and the apical approach, among which the femoral artery approach has the advantage of a convenient operation and fewer complications, thus accounting for more than 90% of the approaches. Under the usual circumstances, patients accepting TAVR treatment may have atherosclerosis, calcification, and even, in severe cases, porcelain aorta. These patients are prone to develop vascular complications and other serious consequences when undergoing TAVR via the peripheral vascular approach [40]. As a result, simulation using the preprocedural 3D printing model may remind clinicians to perform the balloon expansion first and TAVR later. Ovcharenko et al. [41] used a phantom of the vascular system to simulate all stages of delivery system movement along the vascular bed, and the numerical analysis was used to assess the force arising from the passage of the delivery system. Similarly, Rotman et al. [42] reported a novel benchtop patientspecific arterial replicator designed for testing TAVR and

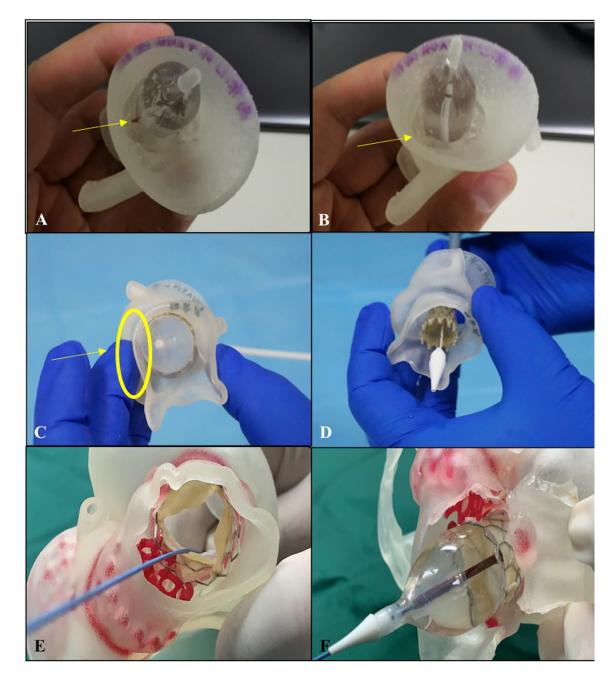


Fig. 5. Prediction of transcatheter aortic valve replacement complications using 3-dimensional printed aortic root models. (A) The 20-mm balloon is expanded in the model; the paravalvular leakage is observed (the yellow arrow). (B) The 23-mm balloon is subsequently expanded in the model, and the paravalvular leakage disappears (the yellow arrow). (C) The yellow circle, which is located between the anterior leaflet of the mitral valve and the membranous part of the interventricular septum, is the possible area of the conduction block. (D) Different sizes of stents are used to ensure the migrated direction of the balloons and then to estimate the position of the conduction block. (E,F) The balloon is expanded *in vitro* to estimate the position of the coronary obstruction.

training interventional cardiologists, which showed the efficacy and reliability in procedural testing. Therefore, 3D printed simulator may be used as an accurate model for surgeons to understand anatomical difficulties and plan procedural strategy.

Discussion and Current Limitations

Studies have shown that among junior residents, selection of a surgical career is most heavily influenced by hands-on participation and positive guidance within a field [11–19,43–45]. Simulation has been used in other fields to provide medical students with early hands-on exposures [46]. The benefits of simulation-based training have been demonstrated by a meta-analysis, the results of which indicated that the training method used could reliably influence outcomes related to trainees' knowledge and skills [47]. Patient-related outcomes could also be influenced by the training method [47].

Schmauss et al. [48] first reported TAVR guided by 3D printing in 2012. Evidence-based studies have clearly suggested the following: First, 3D printing can be used to reconstruct the anatomy of the aortic root realistically, and preprocedural simulations may effectively avoid the complications of TAVR, such as paravalvular leakage, coronary obstruction, and conduction block. Second, the 3D printed models can effectively simulate hemodynamic parameters to provide a more realistic platform in vitro for product testing and development. Finally, the simulations based on the 3D printed models may effectively improve the learning curve. As TAVR continues to improve, 3D printing is being used widely in the development of TAVR, device testing in vitro, simulation training, preprocedural evaluation, and other aspects with the advantages of reconstructed, realistic aortic root anatomical structures. At present, composite materials (such as silicone, resin, polyethylene, and rubber materials with different levels of hardness) are used to print the aortic root model, which can effectively simulate both the elastic valve structures and the rigid calcification structures. In addition, the nature of the 3D printed models enhances a clear understanding of the anatomical structures and minimizes the risk of misunderstandings. The use of simulators has become a way for trainees to practice in a safe, low-pressure environment outside the operating room [49]. Studies have demonstrated that simulators have been remarkably successful in increasing medical students' interest in general surgery and vascular surgery [45,50]. The 3D printed models provide opportunities for simulation of procedures that are not available on other platforms. Simulations are now more commonly incorporated into residency programs to promote improvement of young clinicians [51,52].

However, promoting the teaching and training of TAVR with the guidance of 3D printing may encounter some of the following difficulties: (1) Simulating TAVR is relatively complex because of the specific 3D printing requirements, i.e., a combination of different materials and multiple colors. (2) Teaching and training TAVR guided by 3D printing requires the cooperation of participants from multiple disciplines, a situation that is generally lacking at present. (3) 3D printing machines and materials are expensive. (4) The commercial application of 3D printing in TAVR needs to be expanded.

Future Directions

Cardiovascular Bioprinting

The application of 3D printing in the cardiovascular field is the printing of cardiovascular cells and tissues, known as bioprinting. The material used is bio-ink, not traditional materials. The researchers extracted stem cells from the human body, which were differentiated into different types of other cells, combined with hydrogel matrix and other structures for printing in vitro. Recently, a breakthrough has been made in the research on the strong and tough bonding of hydrogels, the basic principle of which is the synergistic effect of interfacial covalent bond, polymer network topology and adhesive energy dissipation [53]. In addition, various strong hydrogel composites have been prepared to simulate the structure of human tissues [54]. Yang et al. [55] produced heterogeneous hydrogel composites using stereolithography technology, which showed high fatigue resistance.

Personalized Treatment Device

3D printing technology is one of the most important technological breakthroughs of this era. The characteristics of individual customization allow 3D printing to benefit the manufacturing of cardiovascular implants. Guided by the new patient-centered medical model, it is highly possible to introduce 3D printed implants in the cardiovascular field in the future. With the rapid development of 3D printing technology and material science, including the dynamic 4dimensional (4D) printing technology in recent years, on the basis of fully simulating the anatomical structure and function of the aortic valve, dynamic stereoscopic deformation and other features, TAVR treatment devices customized according to the functional characteristics of the anatomical structure of patients will also become an important development trend in the future [56,57]. The promising methods can simulate the performance of a range of bioprosthetic valves in a patient-specific left heart environment, which may be possible to customize the TAVR treatment device to lay the foundation of the methodology.

Fluid Mechanics and Fluid-Structure Coupling

The application of computational fluid dynamics and fluid-structure coupling modeling in the structural and functional evaluation of aortic valve was realized by the integration of 3D printing technology and computer simulation. The inclusion of computational fluid dynamics in a CTderived three-dimensional computational model can evaluate and quantify the pathophysiological status of the aortic valve and specific treatment objectives. The finite element models for simulating the structural dynamics and the fluid structure interaction methods for simulating the performance of bioprosthetic valves may pave the way toward clinically relevant computational models and make it possible to solve important algorithm and model validation challenges that need to be solved in the future. The establishment of this kind of model can also be used to evaluate the influence of the selection of aortic valve interventional therapy instrument types, models and implantation depth on hemodynamics, so as to evaluate and predict the treatment prognosis, including postoperative regurgitation, perioperative complication prediction and patient prognosis assessment, and even future valve durability prediction [58].

Virtual Reality and Holograms

3D printing, combined with virtual reality and hologram technology, is an important progress of digital simulation technology. It is of great help to surgeons to fully understand the details of the structure. In the previous study, Butera et al. [59] reported a holographic augmented reality and 3D printing for surgical management, which could successfully provide the preoperative plan for percutaneous management of abnormal pulmonary venous return. It is a new image mode which is different from the traditional diagnostic image method. In particular, the combination of 4D dynamic image simulation enables surgeons to have a fuller understanding of the structure and function of the aortic root, achieve accurate stereoscopic measurement and dynamic measurement of different phases, and make surgical plan design, instrument type and model selection, and complication prediction more accurate, which is conducive to improving the success rate of surgery, shortening the operation time and improving the prognosis of patients [60].

3D Real-Time Image Fusion

Real-time image fusion technology can assist surgeons in accurate positioning and save operation time. However, the current image fusion technology, no matter 3D CT and fluoroscopy fusion, or 3D ultrasound and fluoroscopy fusion, still has many problems to be solved, including accurate correspondence, dynamic fitting and so on. With the further development of 3D printing and imaging technology and computing technology in the future, there will certainly be more accurate, three-dimensional and higher-fitting operating platforms. Vernikouskaya et al. [61] reported patient-specifically co-registration procedures for image fusion of preprocedural CT datasets with real-time X-ray fluoroscopy during TAVR, which improved the performance of procedures and effectively reduce the procedural time, fluoroscopy times, radiation dose and contrast agents. This will provide more auxiliary support for the operation of the surgeon, especially to obtain ideal intraoperative positioning, surgical design and other visual scenes, so as to benefit more patients.

Artificial Intelligence

The potential adaptability of Artificial intelligence (AI) and Deep learning (DL) simulations to measure key positions in the aortic root makes them likely to be the basis for new technologies to flourish in the future. By integrating a complete heart valve model into preoperative evaluation and simulation, AI can significantly improve the surgeon's confidence in the operation of surgical instruments and the application of intraoperative techniques. In Wang et al.'s [62] study, they developed a novel algorithm which could perform preprocedural assessments by using CT scans and improve evaluation efficiency compared to observers. In the DL framework, AI is applied in intraoperative image processing to allow the computer to evaluate and feedback the quality of medical images obtained automatically and objectively, which is conducive to improving the success rate of surgery and the prognosis of patients [63].

Conclusion

In summary, 3D printed models of the aortic root can realistically reflect its disease states. 3D printing is bound to play a more important role in pre-TAVR simulations due to its significant advantages, especially greater progress will be made in preprocedural training and prediction of complications for surgeons. The use of simulators by young residents and medical students to acquire knowledge and enhance practical experience through educational activities may have an impact on shortening the learning curve.

Availability of Data and Materials

The original contributions presented in the study are included in the article/supplementary material, further inquiries can be directed to the corresponding author.

Author Contributions

YM, YYM and MGZ made substantial contributions to the conception and design of the work; JY and YL made substantial contributions to the design of the work. All authors contributed to editorial changes in the manuscript. All authors read and approved the final manuscript. All authors have participated sufficiently in the work to take public responsibility for appropriate portions of the content and agreed to be accountable for all aspects of the work in ensuring that questions related to its accuracy or integrity.

Ethics Approval and Consent to Participate

Not applicable.

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Conflict of Interest

The authors paid the corresponding amount for each 3D-printed model made by Make Medical Technology Co., Ltd. (Xi'an, China). The authors declare that no conflict of interest between the company and the authors.

Supplementary Material

Supplementary material associated with this article can be found, in the online version, at https://doi.org/10. 59958/hsf.7177.

Video 1. The transcatheter aortic valve replacement pulsatile simulator is used to train main procedures before the operation.

Video 2. The crossing-valve procedure was simulated by surgeons.

Video 3. The TAVR procedures could be simulated by using the model and the simulator vividly, and the accuracy of simulation could be verified by digital subtracted angiography.

References

- Wang C, Zhang L, Qin T, Xi Z, Sun L, Wu H, et al. 3D printing in adult cardiovascular surgery and interventions: a systematic review. Journal of Thoracic Disease. 2020; 12: 3227–3237.
- [2] Jack G, Arora S, Strassle PD, Sitammagari K, Gangani K, Yeung M, et al. Differences in Inpatient Outcomes After Surgical Aortic Valve Replacement at Transcatheter Aortic Valve Replacement

(TAVR) and Non-TAVR Centers. Journal of the American Heart Association. 2019; 8: e013794.

- [3] Mao J, Redberg RF, Carroll JD, Marinac-Dabic D, Laschinger J, Thourani V, et al. Association Between Hospital Surgical Aortic Valve Replacement Volume and Transcatheter Aortic Valve Replacement Outcomes. JAMA Cardiology. 2018; 3: 1070–1078.
- [4] Claessen BE, Tang GHL, Kini AS, Sharma SK. Considerations for Optimal Device Selection in Transcatheter Aortic Valve Replacement: A Review. JAMA Cardiology. 2021; 6: 102–112.
- [5] Corrigan FE, 3rd, Gleason PT, Condado JF, Lisko JC, Chen JH, Kamioka N, *et al.* Imaging for Predicting, Detecting, and Managing Complications After Transcatheter Aortic Valve Replacement. JACC. Cardiovascular Imaging. 2019; 12: 904–920.
- [6] Alasnag MA, Al-Nasser IM, Porqueddu MM, Ahmed WH, Al-Shaibi KF. 3D Model Guiding Transcatheter Aortic Valve Replacement in a Patient with Aortic Coarctation. JACC. Case Reports. 2020; 2: 352–357.
- [7] Bompotis G, Meletidou M, Karakanas A, Sotiriou S, Sachpekidis V, Konstantinidou M, *et al.* Transcatheter Aortic Valve Implantation using 3-D printing modeling assistance. A singlecenter experience. Hellenic Journal of Cardiology: HJC = Hellenike Kardiologike Epitheorese. 2020; 61: 131–132.
- [8] Abd Alamir M, Nazir S, Alani A, Golub I, Gilchrist IC, Jr, Aslam F, et al. Multidetector computed tomography in transcatheter aortic valve replacement: an update on technological developments and clinical applications. Expert Review of Cardiovascular Therapy. 2020; 18: 709–722.
- [9] Levin D, Mackensen GB, Reisman M, McCabe JM, Dvir D, Ripley B. 3D Printing Applications for Transcatheter Aortic Valve Replacement. Current Cardiology Reports. 2020; 22: 23.
- [10] Zelis JM, Meiburg R, Roijen JJD, Janssens KLPM, van 't Veer M, Pijls NHJ, *et al.* 3D-printed stenotic aortic valve model to simulate physiology before, during, and after transcatheter aortic valve implantation. International Journal of Cardiology. 2020; 313: 32–34.
- [11] Gardin C, Ferroni L, Latremouille C, Chachques JC, Mitrečić D, Zavan B. Recent Applications of Three Dimensional Printing in Cardiovascular Medicine. Cells. 2020; 9: 742.
- [12] Ferrari E, Piazza G, Scoglio M, Berdajs D, Tozzi P, Maisano F, et al. Suitability of 3D-Printed Root Models for the Development of Transcatheter Aortic Root Repair Technologies. ASAIO Journal (American Society for Artificial Internal Organs: 1992). 2019; 65: 874–881.
- [13] Ko CY, Escarce JJ, Baker L, Klein D, Guarino C. Predictors for medical students entering a general surgery residency: National survey results. Surgery. 2004; 136: 567–572.
- [14] Berman L, Rosenthal MS, Curry LA, Evans LV, Gusberg RJ. Attracting surgical clerks to surgical careers: role models, mentoring, and engagement in the operating room. Journal of the American College of Surgeons. 2008; 207: 793–800, 800.e1– 800.e2.
- [15] Erzurum VZ, Obermeyer RJ, Fecher A, Thyagarajan P, Tan P, Koler AK, *et al.* What influences medical students' choice of surgical careers. Surgery. 2000; 128: 253–256.
- [16] O'Herrin JK, Lewis BJ, Rikkers LF, Chen H. Why do students choose careers in surgery? The Journal of Surgical Research. 2004; 119: 124–129.
- [17] Akaike M, Fukutomi M, Nagamune M, Fujimoto A, Tsuji A, Ishida K, *et al.* Simulation-based medical education in clinical skills laboratory. The Journal of Medical Investigation: JMI. 2012; 59: 28–35.
- [18] Hosny A, Dilley JD, Kelil T, Mathur M, Dean MN, Weaver JC, et al. Pre-procedural fit-testing of TAVR valves using parametric modeling and 3D printing. Journal of Cardiovascular Computed Tomography. 2019; 13: 21–30.
- [19] Nam JG, Lee W, Jeong B, Park EA, Lim JY, Kwak Y, et al. Three-Dimensional Printing of Congenital Heart Disease Mod-

els for Cardiac Surgery Simulation: Evaluation of Surgical Skill Improvement among Inexperienced Cardiothoracic Surgeons. Korean Journal of Radiology. 2021; 22: 706–713.

- [20] Greil GF, Wolf I, Kuettner A, Fenchel M, Miller S, Martirosian P, et al. Stereolithographic reproduction of complex cardiac morphology based on high spatial resolution imaging. Clinical Research in Cardiology: Official Journal of the German Cardiac Society. 2007; 96: 176–185.
- [21] Byrne N, Velasco Forte M, Tandon A, Valverde I, Hussain T. A systematic review of image segmentation methodology, used in the additive manufacture of patient-specific 3D printed models of the cardiovascular system. JRSM Cardiovascular Disease. 2016; 5: 2048004016645467.
- [22] Halliburton S, Arbab-Zadeh A, Dey D, Einstein AJ, Gentry R, George RT, *et al.* State-of-the-art in CT hardware and scan modes for cardiovascular CT. Journal of Cardiovascular Computed Tomography. 2012; 6: 154–163.
- [23] Vukicevic M, Mosadegh B, Min JK, Little SH. Cardiac 3D Printing and its Future Directions. JACC. Cardiovascular Imaging. 2017; 10: 171–184.
- [24] Li K, Kui C, Lee E, Ho C, Sunny Hei S, Wu W, et al. The Role of 3D Printing in Anatomy Education and Surgical Training: A Narrative Review. MedEdPublish: Dundee, UK. 2017.
- [25] Ma Y, Ding P, Li L, Liu Y, Jin P, Tang J, *et al.* Threedimensional printing for heart diseases: clinical application review. Bio-design and Manufacturing. 2021; 4: 675–687.
- [26] Valverde I. Three-dimensional Printed Cardiac Models: Applications in the Field of Medical Education, Cardiovascular Surgery, and Structural Heart Interventions. Revista Espanola De Cardiologia (English Ed.). 2017; 70: 282–291.
- [27] Wang DD, Gheewala N, Shah R, Levin D, Myers E, Rollet M, et al. Three-Dimensional Printing for Planning of Structural Heart Interventions. Interventional Cardiology Clinics. 2018; 7: 415– 423.
- [28] Maragiannis D, Jackson MS, Igo SR, Schutt RC, Connell P, Grande-Allen J, *et al.* Replicating Patient-Specific Severe Aortic Valve Stenosis with Functional 3D Modeling. Circulation. Cardiovascular Imaging. 2015; 8: e003626.
- [29] Ventola CL. Medical Applications for 3D Printing: Current and Projected Uses. P & T: a Peer-reviewed Journal for Formulary Management. 2014; 39: 704–711.
- [30] Petrini C. Ethical and legal considerations regarding the ownership and commercial use of human biological materials and their derivatives. Journal of Blood Medicine. 2012; 3: 87–96.
- [31] Olivieri LJ, Krieger A, Loke YH, Nath DS, Kim PCW, Sable CA. Three-dimensional printing of intracardiac defects from three-dimensional echocardiographic images: feasibility and relative accuracy. Journal of the American Society of Echocar-diography: Official Publication of the American Society of Echocardiography. 2015; 28: 392–397.
- [32] Hermsen JL, Burke TM, Seslar SP, Owens DS, Ripley BA, Mokadam NA, et al. Scan, plan, print, practice, perform: Development and use of a patient-specific 3-dimensional printed model in adult cardiac surgery. The Journal of Thoracic and Cardiovascular Surgery. 2017; 153: 132–140.
- [33] Bauer T, Linke A, Sievert H, Kahlert P, Hambrecht R, Nickenig G, et al. Comparison of the effectiveness of transcatheter aortic valve implantation in patients with stenotic bicuspid versus tricuspid aortic valves (from the German TAVI Registry). The American Journal of Cardiology. 2014; 113: 518–521.
- [34] Qian Z, Wang K, Liu S, Zhou X, Rajagopal V, Meduri C, et al. Quantitative Prediction of Paravalvular Leak in Transcatheter Aortic Valve Replacement Based on Tissue-Mimicking 3D Printing. JACC. Cardiovascular Imaging. 2017; 10: 719– 731.
- [35] Reiff C, Zhingre Sanchez JD, Mattison LM, Iaizzo PA, Garcia

S, Raveendran G, *et al.* 3-Dimensional printing to predict paravalvular regurgitation after transcatheter aortic valve replacement. Catheterization and Cardiovascular Interventions: Official Journal of the Society for Cardiac Angiography & Interventions. 2020; 96: E703–E710.

- [36] Thorburn C, Abdel-Razek O, Fagan S, Pearce N, Furey M, Harris S, *et al.* Three-dimensional printing for assessment of paravalvular leak in transcatheter aortic valve implantation. Journal of Cardiothoracic Surgery. 2020; 15: 211.
- [37] Rocatello G, El Faquir N, De Santis G, Iannaccone F, Bosmans J, De Backer O, *et al.* Patient-Specific Computer Simulation to Elucidate the Role of Contact Pressure in the Development of New Conduction Abnormalities After Catheter-Based Implantation of a Self-Expanding Aortic Valve. Circulation. Cardiovas-cular Interventions. 2018; 11: e005344.
- [38] Heitkemper M, Hatoum H, Azimian A, Yeats B, Dollery J, Whitson B, *et al.* Modeling risk of coronary obstruction during transcatheter aortic valve replacement. The Journal of Thoracic and Cardiovascular Surgery. 2020; 159: 829–838.e3.
- [39] Young L, Harb SC, Puri R, Khatri J. Percutaneous coronary intervention of an anomalous coronary chronic total occlusion: The added value of three-dimensional printing. Catheterization and Cardiovascular Interventions: Official Journal of the Society for Cardiac Angiography & Interventions. 2020; 96: 330– 335.
- [40] Yokoyama Y, Sakata T, Mikami T, Misumida N, Scotti A, Takagi H, *et al.* Vascular access for transcatheter aortic valve replacement: A network meta-analysis. Journal of Cardiology. 2023; 82: 227–233.
- [41] Ovcharenko EA, Klyshnikov KU, Shilov AA, Kochergin NA, Rezvova MA, Belikov NV, *et al.* Mechanism of Vascular Injury in Transcatheter Aortic Valve Replacement. Sovremennye Tekhnologii V Meditsine. 2021; 13: 6–13.
- [42] Rotman OM, Kovarovic B, Sadasivan C, Gruberg L, Lieber BB, Bluestein D. Realistic Vascular Replicator for TAVR Procedures. Cardiovascular Engineering and Technology. 2018; 9: 339–350.
- [43] Vaporciyan AA, Reed CE, Erikson C, Dill MJ, Carpenter AJ, Guleserian KJ, et al. Factors affecting interest in cardiothoracic surgery: Survey of North American general surgery residents. The Journal of Thoracic and Cardiovascular Surgery. 2009; 137: 1054–1062.
- [44] Allen JG, Weiss ES, Patel ND, Alejo DE, Fitton TP, Williams JA, *et al.* Inspiring medical students to pursue surgical careers: outcomes from our cardiothoracic surgery research program. The Annals of Thoracic Surgery. 2009; 87: 1816–1819.
- [45] Cochran A, Melby S, Neumayer LA. An Internet-based survey of factors influencing medical student selection of a general surgery career. American Journal of Surgery. 2005; 189: 742– 746.
- [46] Lee JT, Qiu M, Teshome M, Raghavan SS, Tedesco MM, Dalman RL. The utility of endovascular simulation to improve technical performance and stimulate continued interest of preclinical medical students in vascular surgery. Journal of Surgical Education. 2009; 66: 367–373.
- [47] Cook DA, Hatala R, Brydges R, Zendejas B, Szostek JH, Wang AT, *et al.* Technology-enhanced simulation for health professions education: a systematic review and meta-analysis. JAMA. 2011; 306: 978–988.
- [48] Schmauss D, Schmitz C, Bigdeli AK, Weber S, Gerber N, Beiras-Fernandez A, *et al.* Three-dimensional printing of models for preoperative planning and simulation of transcatheter valve replacement. The Annals of Thoracic Surgery. 2012; 93: e31– e33.
- [49] Gordon JA, Wilkerson WM, Shaffer DW, Armstrong EG. "Practicing" medicine without risk: students' and educators' responses to high-fidelity patient simulation. Academic Medicine:

Journal of the Association of American Medical Colleges. 2001; 76: 469–472.

- [50] Lee JT, Son JH, Chandra V, Lilo E, Dalman RL. Long-term impact of a preclinical endovascular skills course on medical student career choices. Journal of Vascular Surgery. 2011; 54: 1193–1200.
- [51] Tavakol M, Mohagheghi MA, Dennick R. Assessing the skills of surgical residents using simulation. Journal of Surgical Education. 2008; 65: 77–83.
- [52] Fann JI, Caffarelli AD, Georgette G, Howard SK, Gaba DM, Youngblood P, et al. Improvement in coronary anastomosis with cardiac surgery simulation. The Journal of Thoracic and Cardiovascular Surgery. 2008; 136: 1486–1491.
- [53] Yang J, Bai R, Chen B, Suo Z. Hydrogel adhesion: a supramolecular synergy of chemistry, topology, and mechanics. Advanced Functional Materials. 2020; 30, 1901693.
- [54] Zhao X. Multi-scale multi-mechanism design of tough hydrogels: building dissipation into stretchy networks. Soft Matter. 2014; 10: 672–687.
- [55] Yang H, Ji MK, Yang M, Shi MXZ, Pan YD, Zhou YF, et al. Fabricating hydrogels to mimic biological tissues of complex shapes and high fatigue resistance. Matter. 2021; 4: 1935–1946.
- [56] Votta E, Le TB, Stevanella M, Fusini L, Caiani EG, Redaelli A, et al. Toward patient-specific simulations of cardiac valves: state-of-the-art and future directions. Journal of Biomechanics. 2013; 46: 217–228.
- [57] de Jaegere P, Rocatello G, Prendergast BD, de Backer O, Van Mieghem NM, Rajani R. Patient-specific computer simulation for transcatheter cardiac interventions: what a clinician needs to know. Heart (British Cardiac Society). 2019; 105: s21–s27.

- [58] Marom G. Numerical methods for fluid-structure interaction models of aortic valves. Archives of Computational Methods in Engineering. 2015; 22: 595–620.
- [59] Butera G, Sturla F, Pluchinotta FR, Caimi A, Carminati M. Holographic Augmented Reality and 3D Printing for Advanced Planning of Sinus Venosus ASD/Partial Anomalous Pulmonary Venous Return Percutaneous Management. JACC. Cardiovascular Interventions. 2019; 12: 1389–1391.
- [60] Sugimoto M. Extended Reality (XR: VR/AR/MR), 3D Printing, Holography, AI, Radiomics, and Online VR Tele-Medicine for Precision Surgery. In Takenoshita S, Yasuhara H (eds.) Surgery and Operating Room Innovation (pp. 65–70). Springer: Singapore. 2021.
- [61] Vernikouskaya I, Rottbauer W, Seeger J, Gonska B, Rasche V, Wöhrle J. Patient-specific registration of 3D CT angiog-raphy (CTA) with X-ray fluoroscopy for image fusion during transcatheter aortic valve implantation (TAVI) increases performance of the procedure. Clinical Research in Cardiology: Official Journal of the German Cardiac Society. 2018; 107: 507–516.
- [62] Wang M, Niu G, Chen Y, Zhou Z, Feng D, Zhang Y, et al. Development and validation of a deep learning-based fully automated algorithm for pre-TAVR CT assessment of the aortic valvular complex and detection of anatomical risk factors: a retrospective, multicentre study. EBioMedicine. 2023; 96: 104794.
- [63] Meyer A, Kofler M, Montagner M, Unbehaun A, Sündermann S, Buz S, *et al.* Reliability and Influence on Decision Making of fully-automated vs. semi-automated Software Packages for Procedural Planning in TAVI. Scientific Reports. 2020; 10: 10746.